#### Cellular/Molecular

# Pacemaker Rate and Depolarization Block in Nigral Dopamine Neurons: A Somatic Sodium Channel Balancing Act

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Midbrain dopamine (DA) neurons are slow intrinsic pacemakers that undergo depolarization (DP) block upon moderate stimulation. Understanding DP block is important because it has been correlated with the clinical efficacy of chronic antipsychotic drug treatment. Here we describe how voltage-gated sodium ( $Na_V$ ) channels regulate DP block and pacemaker activity in DA neurons of the substantia nigra using rat brain slices. The distribution, density, and gating of  $Na_V$  currents were manipulated by blocking native channels with tetrodotoxin and by creating virtual channels and anti-channels with dynamic clamp. Although action potentials initiate in the axon initial segment and  $Na_V$  channels are distributed in multiple dendrites, selective reduction of  $Na_V$  channel activity in the soma was sufficient to decrease pacemaker frequency and increase susceptibility to DP block. Conversely, increasing somatic  $Na_V$  current density raised pacemaker frequency and lowered susceptibility to DP block. Finally, when  $Na_V$  currents were restricted to the soma, pacemaker activity occurred at abnormally high rates due to excessive local subthreshold  $Na_V$  current. Together with computational simulations, these data show that both the slow pacemaker rate and the sensitivity to DP block that characterizes DA neurons result from the low density of somatic  $Na_V$  channels. More generally, we conclude that the somatodendritic distribution of  $Na_V$  channels is a major determinant of repetitive spiking frequency.

#### Introduction

Substantia nigra (SN) dopamine (DA) neurons exhibit slow intrinsic pacemaker activity (Kita et al., 1986; Hainsworth et al., 1991). Although voltage-gated calcium channels have been implicated in driving pacemaker activity (Nedergaard et al., 1993; Mercuri et al., 1994; Chan et al., 2007; Puopolo et al., 2007; Putzier et al., 2009a), voltage-gated sodium (Na<sub>V</sub>) channels also contribute to the slow depolarization (DP) phase leading to action potential (AP) initiation (Puopolo et al., 2007). Furthermore, Na<sub>V</sub> channels are responsible for the initiation of APs in the axon initial segment (AIS) and their subsequent propagation in the axon, dendrites, and soma, which in turn triggers DA release from terminals and dendrites (Grace and Bunney, 1983b; Santiago et al., 1992; Häusser et al., 1995; Gentet and Williams, 2007; Blythe et al., 2009). Thus, Na<sub>V</sub> channels are major determinants of nigral DA neuron activity and function.

Interestingly, the efficacy of antipsychotic drugs is correlated with induction of chronic DP block in DA neurons

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(Chiodo and Bunney, 1983; White and Wang, 1983a,b; Grace and Bunney, 1986; Esposito and Bunney, 1989; Skarsfeldt and Perregaard, 1990; Skarsfeldt, 1992; Valenti et al., 2011). With acute excitation, DP block is preceded by attenuation of AP amplitude, broadening of each successive spike, and the eventual failure of AP production (Richards et al., 1997; Blythe et al., 2009). A computational modeling study of DA neurons suggested that DP block may result from cumulative inactivation of Na<sub>v</sub> channels leading to an increase in AP threshold that eventually becomes so depolarized that APs cannot initiate (Kuznetsova et al., 2010). However, this model, which did not take into account that in DA neurons APs propagate from the AIS through a dendrite into the soma, has not been tested experimentally. Thus, it is not known whether Na<sub>V</sub> channels in the AIS and/or soma determine susceptibility to DP block in intact SN DA neurons.

Here the role of  $Na_V$  channels in SN DA neuron activity is investigated by manipulating  $Na_V$  current magnitude, distribution, and gating with the dynamic clamp, a device that adds virtual channels via computationally generated currents injected through a patch pipette into the neuron. Specifically, virtual  $Na_V$  conductance, which was based on native SN DA neuron currents characterized in nucleated patches (Seutin and Engel, 2010), was added or subtracted from the soma of SN DA neurons in the brain slice. Even though APs initiate in the AIS, somatic  $Na_V$  channels are shown to control the bal-

Received March 13, 2012; revised Aug. 9, 2012; accepted Aug. 17, 2012.

Author contributions: K.R.T., J.P.H., C.C.C., and E.S.L. designed research; K.R.T., M.A.H., and C.C.C. performed research; K.R.T., M.A.H., J.P.H., and E.S.L. analyzed data; K.R.T., J.P.H., C.C.C., and E.S.L. wrote the paper.

This work was supported by National Institutes of Health Grants R01NS061097 and F32NS078994. The authors declare no competing financial interests.

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ance between pacemaker frequency and susceptibility to DP block in nigral DA neurons.

#### Materials and Methods

Solutions and reagents. Sucrose modified artificial CSF (s-ACSF) contained the following (in mM): 87 NaCl, 75 sucrose, 2.5 KCl, 25 NaHCO<sub>3</sub>, 1.25 NaH<sub>2</sub>PO<sub>4</sub>, 0.5 CaCl<sub>2</sub>, 7 MgSO<sub>4</sub>, 25 glucose, 0.15 ascorbic acid, and 1 kynurenic acid, pH 7.4. Normal ACSF contained the following (in mM): 124 NaCl, 4 KCl, 25.7 NaHCO<sub>3</sub>, 1.25 NaH<sub>2</sub>PO<sub>4</sub>, 2.45 CaCl<sub>2</sub>, 1.2 MgSO<sub>4</sub>, 11 glucose, and 0.15 ascorbic acid, pH 7.4. Adult perfusion and brain slice solution contained the following (in mM): 105 N-methyl-D-glucamine-Cl, 105 HCl, 2.5 KCl, 1.2 NaH<sub>2</sub>PO<sub>4</sub>, 26 NaHCO<sub>3</sub>, 25 glucose, 10 MgSO<sub>4</sub>, 0.5 CaCl<sub>2</sub>, 5 ascorbic acid, 3 sodium pyruvate, 2 thiourea, and 1 kynurenic acid, pH 7.4. The pipette solution contained the following (in mM): 120 potassium gluconate, 20 KCl, 10 HEPES, 2 MgCl<sub>2</sub>, 0.1 EGTA, and 1.2 ATP disodium salt, pH 7.3. All salts were purchased from either Sigma-Aldrich or Thermo-Fisher Scientific. Tetrodotoxin with citrate was purchased from Alomone Labs.

*Midbrain slice preparation*. All experiments were conducted according to University of Pittsburgh Institutional Animal Care and Use Committee approved protocols. Midbrain slice preparations from postnatal days 14–21 (P14–P21) male Sprague Dawley rats (Hilltop Laboratories) were performed as previously described (Putzier et al., 2009b). A small subset of experiments was performed in slices from P42 male Sprague Dawley rats. These older rats were anesthetized with isoflurane, transcardially perfused with ice-cold carbogenated adult perfusion solution and decapitated (Peça et al., 2011; Ting and Feng, 2011). The brain was then

quickly removed and placed into ice-cold, carbogenated s-ACSF for P14–P21 rats and ice-cold, carbogenated adult slice solution for P42 rats. Coronal midbrain slices ( $250 \ \mu m$ ) were cut using a Vibratome 3000 (The Vibratome Company) in the respective ice-cold, carbogenated solutions. Midbrain slices from P14–P21 rats were incubated in room temperature carbogenated s-ACSF in an interface chamber for at least 1 h and then held in room temperature normal ACSF in the interface chamber until use. Midbrain slices from P42 rats were incubated in room-temperature carbogenated adult slice solution in an interface chamber for 30 min, during which time the adult slice solution was slowly replaced by the room-temperature carbogenated normal ACSF (Peça et al., 2011; Ting and Feng, 2011). These slices were then maintained for at least another 30 min in room temperature normal ACSF in the interface chamber before use.

*Electrophysiology*. Patch electrodes were fabricated from Corning 7056 Patch Glass (Warner Instruments) and coated near the tip with beeswax to reduce the pipette capacitance. Carbogenated normal ACSF was used for bath perfusion of midbrain slices at a rate of 2 ml/min. SN pars compacta DA neurons were identified by location and electrophysiological characteristics as described previously (Grace and Bunney, 1983a; Lacey et al., 1989; Richards et al., 1997).

Dynamic clamp is a modified current-clamp technique that creates virtual channels in a living cell by dynamically adjusting the current injected in response to real-time changes in the membrane potential based on previously modeled channel behavior. The virtual NMDA receptor (NMDAR) conductance in the present experiments used equations from previous dynamic clamp studies of DA neurons (Deister et al., 2009; Putzier et al., 2009a). Because the virtual Na<sub>v</sub> channel was based on



**Figure 1.** Sodium channel and SN DA neuron model descriptions. **A**, Comparison of the peak Na<sub>V</sub> current/voltage response measured from SN DA neuron nucleated patches by Seutin and Engel (2010) (circles) and the modeled Na<sub>V</sub> current/voltage response based on fitting those data (squares and line). **B**, Steady-state inactivation ( $h_{\infty}$ ; solid line) and activation ( $m_{\infty}^3$ ; dashed line) curves of the model Na<sub>V</sub> current used in both dynamic clamp and modeling experiments. **C**, SN DA neuron compartmental model description. Left, Morphology of modeled SN DA neuron. Soma and distal dendritic recording sites are located by arrows. No axon is shown. Middle, Somatic currents flowing during the interspike interval (ISI).  $I_{KV}$  = composite voltage-gated potassium currents,  $I_b$  = sum of constitutively active GIRK current and sodium leak current,  $I_{Cav,L}$  = L-type calcium current,  $I_{Nav}$  = TTX-sensitive voltage-gated sodium current, and  $I_{Axial}$  = current flowing out of the soma into the central compartment of the dendrite. Right, Simulated pacing activity of the model neuron as measured from the soma (top trace) and a single AP (bottom trace). Scale indicated below each trace.

Table '	1. Time and	voltage de	pendence of	f model gatiı	ng variables

x	$x_{half}$ (mV)	$x_k$ (mV)	Time constants: tau <sub>x</sub> (ms)
m	-30.0907	9.7264	0.01 + 1/(a + b), a = -(15.6504 + 0.4043 V)/
			[exp(−19.565 − 0.50542 v) − 1]
			$b = 3.0212 \exp(-7.4630 \times 10^{-3} v)$
h <sub>f</sub>	-54.0289	-10.7665	$0.4 + 1/(a + b), a = 5.0754 \times 10^{-4} \exp(-6.3213 \times 10^{-2} v)$
			$b = 9.7529 \exp(0.13442 v)$
h <sub>s</sub>	-54.0289	-10.7665	$0.4 + 1/(a + b), a = 1.3134 \times 10^{-2} \exp(8.5636 \times 10^{-4} v)$
			$b = 13.165 \exp(0.14556 v)$
п	-25	12	$1 + 10\exp(-\{\ln[1 + 0.05 (\nu + 40)]/0.05\}^2/300)$
1	-40	10	1/(a + b), a = -0.020876(v + 39.726)/(exp((v + 39.726)/))
			4.711) — 1)
			$b = 0.19444 \exp(-(v + 15.338)/224.21)$

nucleated-patch voltage-clamp recordings at 25°C (Seutin and Engel, 2010), all recordings were performed at 25°C.

Whole-cell recordings in the current-clamp and dynamic clamp configurations were performed as previously described (Kullmann et al., 2004; Putzier et al., 2009b). Briefly, the current-clamp and dynamic clamp recording system included an A-M Systems Patch-Clamp Amplifier Model 2400 (National Instruments), a National Instruments PXI-1002 CPU for real-time loop computation, and an IBM MT-M 8310-47U CPU with Pentium 4 processor used for user-G-clamp interface. LabVIEW-RT 8.1 (National Instruments) was used to run the G-clamp 2.02 software (http://hornlab.neurobio.pitt. edu). Current-clamp and dynamic clamp measurements were performed with a feedback loop rate of 20 kHz, which has been



**Figure 2.** Inward currents of the AIS and soma are reduced during DP block induction. Representative recordings from SN DA neurons current-clamped at -60 mV followed by (**A**) a 2 s, 250 pA current injection and (**B**) a 5 s dynamic clamp application of 30 nS of virtual NMDAR conductance to induce DP block. **C**, The first, fourth, and last APs (top of the example trace in **A**) and their corresponding dV/dt (middle) and phase plane (bottom) plots. **D**, The APs (top) in the first position, at 1 s of stimulation, at 2 s of stimulation, and in the last position of the example trace in **B** and their corresponding dV/dt (middle) and phase plane (bottom) plots. The arrows in **C** indicate the peak net current flowing during the AIS and somatic portions of the AP. An upward deflection indicates a net inward current and a downward deflection indicates a net outward current. Peak AIS and somatic dV/dt for (**D**) current injection and (**F**) virtual NMDA-induced DP block. Error bars indicate the mean  $\pm$  SEM (for current injection n = 9; for NMDA n = 7).

#### Table 2. Quantification of AP and inward current changes during DP block development

	AP position	AP peak (mV)	AP AHP (mV)	AP threshold (mV)	Peak AIS <i>dV/dt</i> (V/s)	Peak somatic <i>dV/dt</i> (V/s)
Current	1st	26.5 ± 1.4	$-56.5\pm1.3$	$-40.8\pm1.8$	59.4 ± 5.8	125.7 ± 9.0
<i>n</i> = 9	4th				$47.3\pm4.4$	$73.6\pm5.9$
	Last	$13.8\pm3.3$	$-48.9\pm1.1$	$-31.5\pm1.7$	$33.2\pm5.4$	$46.9\pm7.3$
gNMDA	1st	$28.0\pm1.4$	$-60.2\pm1.8$	$-41.4\pm1.2$	$65.2\pm5.0$	$141.3 \pm 12.1$
<i>n</i> = 7	1 s				$41.4\pm4.5$	$61.7\pm8.8$
	2 s				$30.4\pm2.7$	$38.3\pm5.3$
	Last	11.8 ± 2.7	$-53.8 \pm 2.7$	$-26.7 \pm 1.4$	$26.9\pm3.7$	$32.8 \pm 9.4$

previously shown to be sufficient for fast  $Na_V$  conductances (Kullmann et al., 2004; Bettencourt et al., 2008).

The mean and SEM pipette, series and membrane resistances were  $3.34 \pm 0.09$ ,  $12.92 \pm 0.96$ , and  $218.7 \pm 8.8 M\Omega$ , respectively, for 91 recordings before compensation. Series resistance was monitored throughout each experiment and compensated using the bridge circuitry of the amplifier. The average membrane capacitance was  $149.2 \pm 3.9$  pF for 91 cells. Only cells that were spontaneously active after breaking through to the whole-cell configuration and before tetrodotoxin (TTX) treatment were included in the results presented here. Furthermore, dynamic clampinduced changes in activity were reversible.

In the current-clamp recordings, SN DA neurons were held at -60 mV with bias current to prevent spontaneous pacing in between 2 s, 50 pA current steps from -100 to 300 pA with a 7 s interpulse interval. With this paradigm, the characteristic sag in the membrane potential in response to hyperpolarization, slow pacemakerlike activity with small DPs, and DP block with larger DPs could be monitored before and after treatment. Synaptic conductance-induced DP block was elicited by current-clamping the membrane potential to -60 mV and adding 30 nS of virtual NMDA conductance for 5 s with dynamic clamp. In some experiments, virtual channels or current steps were added to freely pacing neurons.

Whole-cell voltage-clamp recordings were performed to determine the amount of time needed for full block of Na<sub>V</sub> channels by 1  $\mu$ M TTX in this midbrain slice preparation. Although voltage-clamp recording from intact neurons in slices is limited by incomplete space clamp, these recordings were used only to determine the time course of TTX action, not current kinetics. Normal ACSF was supplemented with 2 mM CoCl<sub>2</sub> and 15 mM TEA-Cl, and K gluconate and KCl were replaced by 140 mM CsCl in the pipette solution to block voltage-sensitive potassium and calcium currents. The cells were held at -60 mV and stepped to -40 mV every 30 s. After 2 min of baseline recording, 1 µM TTX was superfused across the slice and the peak current amplitude was monitored until stable. The average time for complete block of sodium current was  $6.6 \pm 1.0 \text{ min}$  (range from 5 to 9 min). Therefore, in current and dynamic clamp recordings in which 1  $\mu$ M or 10 nM TTX was used, the slices were superfused for at least 10 min or 20 min, respectively, to ensure steady-state block.

Data analysis. AP characteristics and firing

frequencies were measured and dV/dt and phase plane analysis were conducted with IGOR Pro 5.05A (WaveMetrics) with the NeuroMatic v 2.00 plug-in (http://www.neuromatic.thinkrandom.com/index.html). AP height was measured from the AP peak to the trough of the afterhyperpolarization (AHP). AP threshold was measured from phase plane plots. Evoked AP frequency was measured from the peak of the first AP to the peak of the last AP during a stimulus. AP frequency during pacemaking was measured for a defined duration.

Virtual sodium channel description. The description of the  $Na_V$  current kinetics used in both the modeling and dynamic clamp experiments was derived from rat SN DA nucleated patch voltage-clamp recordings pub-

lished by Seutin and Engel (2010). The Seutin and Engel voltage dependence of activation (m) and inactivation  $(h_f)$  of the SN DA neuron Nav current assumed a Goldman-Hodgkin-Katz driving force and that no inactivation occurs before current peak. Those data were refitted because the dynamic clamp implementation used an ohmic drive, and at certain voltage ranges, the time scales for the activation and inactivation are not clearly separated. A slow component of inactivation  $(h_s)$  was added to fit the data at -120 mV where two components of inactivation were clearly observed by Seutin and Engel (2010). Figure 1A compares the Nav current-voltage relationships from Seutin and Engel's experimental data and the modeled/virtual Nav current. Table 1 summarizes the time and voltage-dependent gating variables calculated for the SN DA neuron Nav current and Figure 1 B shows the resulting voltage dependence of steady-state activation and inactivation for the modeled/virtual Nav channel.

Compartmental model. The SN DA neuron model was implemented in the NEURON simulation package (Hines and Carnavale, 1997) using a real DA neuron morphology (Vetter et al., 2001) downloaded from the neuromorpho. org database (Fig. 1C, left). Unless otherwise indicated, all compartments had the same conductance densities, in agreement with Häusser et al. (1995), who found similar fast sodium conductance on the soma and dendrites. The simulated membrane currents included: (1) the constitutively active GIRK conductance (Bradaia et al., 2009) and a sodium leak (Khaliq and Bean, 2010), which contribute to the net background current  $(I_b)$ , (2) an L-type calcium conductance (I<sub>Cav,L</sub>) (Durante et al., 2004), (3) a composite potassium conductance  $(I_{K\nu})$ (Ding et al., 2011), and (4) the TTX-sensitive

sodium conductance  $(I_{\text{Nav}})$  (Seutin and Engel, 2010) as described above. The currents in the model are given by  $I_b = g_{\text{girk}}(v + 85)/(1 + \exp((v + 45)/20)) + g_{\text{Naleak}}(v - 60), I_{\text{Nav}} = g_{\text{Nav}}m^3(h_f + h_s)(v - 60), I_{Kv} = g_Kn^3(v + 85), \text{ and } I_{\text{Cav,L}} = g_{\text{Cav,L}} l(v - 60), \text{ where the gating variables } m, h_f, h_s, n, and l obey equations of the form <math>dx/dt = (x_{\text{inf}} - x)/\tan x$  with  $x_{\text{inf}} = [1 + \exp(-(v - x_{\text{half}})/x_k)]^{-1}$ . Maximal conductances in  $\mu$ S/cm<sup>2</sup> were  $g_{\text{Nav}} = 3930, g_{Kv} = 3000, g_{\text{Cav,L}} = 20.8, g_{\text{girk}} = 226, \text{ and } g_{\text{Na,leak}} = 33.75$ . Values for  $x_{\text{half}} x_k$ , and tau<sub>x</sub> are given in Table 1. The resulting interspike interval (ISI) currents are modeled in Figure 1*C* (middle).

The axial resistivity was 200 ohm cm and the capacitance was 1  $\mu$ F/ cm<sup>2</sup>. The passive properties of the model were calibrated by confirming that when the neuron was held at -60 mV via current-clamp in the soma, additional small current pulses caused a change in somatic membrane potential to be reduced by  $\sim$ 20% at a distance of 200  $\mu$ m from the soma along a primary dendrite (i.e., in agreement with Häusser et al., 1995). Some simulations were performed with a fixed 50  $\mu$ s time step (sampling rate in dynamic clamp slice recordings) for the simulated dynamic clamp current injection only and a variable step size CVODE algorithm with small error tolerance for all other differential equations. These results (data not shown) were qualitatively similar to the ones reported in the text with variable step size updating for all state variables. Under these conditions, this model neuron was able to successfully replicate the characteristic slow pacemaker activity and broad APs of SN DA neurons (Fig. 1*C*, right).

Alternative models. Two other model neurons were created for comparison to the reduced somatodendritic model depicted in Figure 1. The first contained an axon coming off a dendrite that was composed of the same currents as the rest of the somatodendritic com-



**Figure 3.** Reduction of AIS and somatic  $Na_v$  current increases susceptibility to DP block. *A*, Representative APs (top) from a SN pars compacta DA neuron current-clamp recording in response to a 75 pA current injection before (control) and 20 min after 10 nm TTX application (10 nm TTX) and their corresponding *dV/dt* (middle) and phase plane (bottom) plots. *B*, Representative current-clamp recordings before (control) and after 10 nm TTX application (10 nm TTX) in response to a 5 s, 75 pA current injection during normal pacing. *C*, Resistance to DP block as quantified by length of activity divided by the stimulus length plotted against the stimulus amplitude before (circles; control) and after 10 nm TTX (squares) application. Symbols and error bars indicate the mean  $\pm$  SEM for five cells.

partments except that the Na<sub>V</sub> conductance in the axon was three times larger than in the soma, and the GIRK conductance was 1.11 times larger than in the soma. As little is known about the density, distribution, and composition of channels in SN DA neuron axons or AISs, these values were speculative and selected for their ability to produce natural pacemaker-like activity. The second model neuron was the same as described in Figure 1 with the addition of a calcium-activated SK potassium channel current and a calcium balance system (i.e., calcium buffering and pumping). When these models were compared with the reduced somatodendritic model of Figure 1, they were found to produce similar responses under identical experimental paradigms. Therefore, since the responses from the three models were similar and the currents defining the reduced model were better established, the reduced model simulations were reported here.

#### Results

#### DP block by inhibition of native Nav channels

To induce DP block, SN DA neurons were current-clamped to -60 mV and then depolarized by either a 250 pA current injection or addition of 30 nS of virtual NMDAR conductance generated by the dynamic clamp (Fig. 2*A*, *B*). Each stimulus induced APs that attenuated progressively (i.e., peak values dropped while AHPs and thresholds became depolarized) until activity ceased (Fig. 2*A*–*D*; Table 2). Current (*I*) flowing during these responses is evident from dV/dt because  $dV/dt = -I/C_m$ , where  $C_m$  equals membrane capacitance. Specifically, because APs in DA neurons initiate in the AIS and backpropagate into the soma, plotting dV/dt versus time or membrane



**Figure 4.** Addition of somatic Na<sub>v</sub> current decreases susceptibility to DP block induced by distributed submaximal Na<sub>v</sub> block. *A*, Representative APs (top) from an SN DA neuron current-clamp recording in response to a 75 pA current injection 20 min after 10 nm TTX application (10 nm TTX; Fig. 2 *A*) and with 100 nS of virtual Na<sub>v</sub> added back to the soma with dynamic clamp (10 nm TTX + 10 nS gNa<sub>v</sub>) and their corresponding *dV/dt* (middle) and phase plane (bottom) plots. *B*, Current-clamp recording from the same cell represented in Figure 2 *B* after 10 nm TTX application with the addition of 100 nS (top) and 200 nS (bottom) of virtual Na<sub>v</sub> channel conductance applied throughout recording and responses to 5 s, 75 pA current injections. *C*, Resistance to DP block as quantified by length of activity divided by the stimulus length plotted against the stimulus amplitude after 10 nm TTX alone (squares; Fig. 2*C*), with the addition of 100 nS (open circles), and 200 nS (triangles) of virtual Na<sub>v</sub> channel conductance. Symbols and error bars indicate the mean  $\pm$  SE of 3–5 cells.

potential reveals two inward current components during the upstroke of the AP: initial activation of  $Na_V$  channels in the AIS and subsequent  $Na_V$  channel activation in the soma (Fig. 2*C*,*D*, middle and bottom). During development of DP block induced either by current injection or virtual NMDARs, both the AIS and somatic  $Na_V$  currents revealed by dV/dt plots progressively decreased (Fig. 2*C*–*F*; Table 2).

To determine whether the reduction of Na<sub>V</sub> channel activity is sufficient to increase susceptibility to DP block, a submaximal concentration (10 nM) of TTX was bath applied to the slice and SN DA neurons were depolarized with small current injections. At this dose, the Na<sub>V</sub> channel blocker slowed intrinsic pacemaker activity from  $0.92 \pm 0.09$  Hz to  $0.49 \pm 0.22$  Hz (n = 5) and reduced AP amplitude from  $88.9 \pm 4.5$  to  $74.7 \pm 8.3$  mV (n = 5). The latter effect was also evident in the first AP evoked following current injection, which also had a slower rise time and a more depolarized threshold (Fig. 3A, top). dV/dt plots revealed that TTX reduced both the AIS and somatic Na<sub>V</sub> currents by onethird (Fig. 3A): AIS peak dV/dt dropped from  $38.8 \pm 6.2$  to  $23.4 \pm 3.7$  V/s and somatic peak dV/dt dropped from  $94.5 \pm 14.8$ to  $59.2 \pm 6.1$  V/s (n = 4). Partial block of AIS and somatic channels also changed the response to current injection. For example, a 75 pA current injection that induced sustained activity under control conditions induced DP block after 10 nM TTX (Fig. 3*B*). A variety of current injections showed that concurrent TTXinduced inhibition of Na<sub>V</sub> channels in the AIS and soma reduced the duration of activity evoked by current injection (Fig. 3*C*). Therefore, global partial inhibition of Na<sub>V</sub> channels increases the susceptibility of SN DA neurons to DP block.

### Addition of virtual Na<sub>v</sub> channels to the soma delays DP block

The contribution of somatic Nav channels to DP block was then examined by adding virtual Nav channels with the dynamic clamp to the soma (i.e., the position of the patch pipette passing current from the dynamic clamp). After 20 min of 10 nM TTX application, somatic virtual Nav channels altered the first AP evoked by a 75 pA current injection in currentclamped neurons: addition of somatic virtual Nav channels increased AP height and the somatic component of the dV/dtplot without changing threshold or the AIS component of the dV/dt plots (Fig. 4A). In this example, addition of 100 nS of virtual Nav conductance nearly replaced the native Nav channels blocked by TTX in the soma, but had no effect in the AIS (compare Figs. 3A, 4A). Strikingly, this soma-specific manipulation prevented DP block in this neuron (compare Figs. 3B, 4B). The reduction in susceptibility to DP block was evident with a variety of current injections in independent experiments (Fig. 4C). Furthermore, while 100 nS of somatic virtual Nav channels delayed DP block, 200 nS prevented DP block. There-

fore, the increased sensitivity to DP block produced by pharmacological reduction of  $Na_V$  channel activity in both the soma and AIS is reversed by adding  $Na_V$  channels solely to the soma.

The impact of adding virtual  $Na_V$  channels to the soma was also evident in the absence of TTX and in both adolescent (P14– P21) and older (P42) animals. Specifically, when DP block was induced by current injection or addition of virtual NMDARs (Fig. 2), addition of 100 nS of virtual  $Na_V$  channels to the soma delayed DP block, while adding 200 nS of  $Na_V$  channel conductance produced sustained activity (Fig. 5). Therefore, in the absence of pharmacological inhibition and regardless of age, increasing somatic  $Na_V$  channel number is sufficient to diminish susceptibility to DP block.

#### Somatic virtual anti-Nav channels promote DP block

Dynamic clamp can also be used to add virtual anti-Na<sub>V</sub> channels to counterbalance the activity of native channels in the soma. In these experiments, native somatic channels respond normally to changes in membrane potential, but their depolarizing currents are nullified by current from virtual anti-channels that gate normally, but produce current that flows in the opposite direction. Thus, with this approach, the dynamic clamp produces a net reduction in somatic Nav conductance. The spatial specificity of virtual anti-Na<sub>V</sub> channels was apparent from the AP waveform and dV/dt plots (Fig. 6A): only the somatic component was inhibited by the antichannels. Reducing the somatic  $Na_V$  current in this way hastened DP block induced by current injection by  $51 \pm 18\%$ (n = 5) and by virtual NMDARs by 40  $\pm$ 2.4% (n = 3) (Fig. 6B, C). Together, the responses to virtual Na<sub>V</sub> channels and anti-Na<sub>v</sub> channels (Figs. 5, 6) demonstrate that even though APs initiate in the AIS, somatic Nav channel density controls the susceptibility to DP block.

## Pacemaker rate is proportional to somatic Na<sub>v</sub> channel density

Having implicated somatic Nav channels in DP block, the effects of changing somatic Nav channel density on pacemaker activity of SN DA neurons was evaluated by adding virtual Nav and anti-Na<sub>v</sub> channels to spontaneously pacemaking neurons. Addition of virtual Na<sub>v</sub> channels at the same levels used to delay DP block resulted in increased pacemaker rate (Fig. 7A, B), while reducing the somatic  $Na_V$  current density with virtual anti-Nav channels decreased pacemaker activity (Fig. 7C). Indeed, there was a linear relationship between virtual Nav conductance and pacemaker frequency (Fig. 7D). This relationship reflects that virtual Nav channels contribute a substantial depolarizing current during the ISI (Fig. 7*E*). This contribution fits with the activation curve of rat SN DA Na<sub>v</sub> currents (Fig. 1B, dotted line), the ISI membrane potential of rat SN DA neurons (Fig. 7E, approximately -60 mV to -40 mV) and the previous demonstration that Nav current influences pacemaker activity in mouse nigral DA neurons

(Puopolo et al., 2007). Thus, somatic  $Na_V$  channels coordinately reduce susceptibility to DP block (Figs. 4–6) and enhance pacemaker frequency (Fig. 7).

### Somatic virtual Na $_{\rm v}$ channels alone produce abnormally fast pacemaker activity

The marked effects of somatic  $Na_V$  channels in the presence of native AIS and dendritic  $Na_V$  channels raise the question of whether somatic  $Na_V$  channels alone are sufficient for normal DA neuron pacemaker activity. To address this issue, all native  $Na_V$ channels and APs were blocked with 1  $\mu$ M TTX while currentclamping neurons to -60 mV. Then 2 s long 50 pA current injections were applied to elicit DP (Fig. 8*A*). Finally, various levels of virtual  $Na_V$  conductance were added back to the soma with the dynamic clamp (Fig. 8*A*, bottom two traces) until the



**Figure 5.** Additional somatic Na<sub>V</sub> channels reduce DP block produced by current injection and virtual NMDA conductance in adolescent and older animals. Representative recordings from SN DA neurons current-clamped at -60 mV followed by (*A*) a 2 s, 250 pA current injection and (*B*) a 5 s dynamic clamp application of 30 nS of virtual NMDAR conductance, to induce DP block under control conditions (top) and with 100 nS (middle) or 200 nS (bottom) of virtual NaV added via dynamic clamp. Resistance to DP block as quantified by length of activity divided by the stimulus length plotted against the virtual Na<sub>V</sub> conductance in response to a (*C*) current injection and (*D*) virtual NMDA conductance. Current injections were 250 pA for SN DA neurons in slices from P14–P21 rats (open circles; n = 11) and 200 pA current injection to SN DA neuron in slices from a P42 rat (black square; n = 3). NMDA conductance (30 nS) was used to stimulate SN DA neurons in slices from P14–P21 (open circles; n = 12) and P42 (black squares; n = 3) rats. Symbols and error bars indicate the mean  $\pm$  SEM.

height of the first AP (measured from peak to trough of AHP) began to approach control levels (Fig. 8*A*,*B*).

With the production of large APs, repetitive spiking was evoked with Na<sub>V</sub> channels only in the soma (Fig. 8*A*,*D*). However, this activity was abnormally fast; for example, 800 nS of virtual Na<sub>V</sub> conductance, which produced APs that were ~80% of the control height (Fig. 8*B*), resulted in pacemaker-like activity that was ~3-fold faster than that of the native distributed channel (Fig. 8*C*). Furthermore, somatic virtual channels reconstituted true pacemaker activity (i.e., repetitive spiking without added bias current injection), but spiking frequency was again higher than normal (Fig. 8*D*; n = 11). The production of abnormally high pacemaker rates by somatic restriction of Na<sub>V</sub> channels implies that the widespread distribution of Na<sub>V</sub> channels in the somatodendritic compartment of SN DA neurons is critical for the production of native slow pacemaker activity.



**Figure 6.** Addition of virtual anti-Na<sub>v</sub> channels to the soma hastens DP block. The dynamic clamp technique was used to add 100 nS of virtual anti-Na<sub>v</sub> conductance to the soma of an SN DA neuron while being current-clamped to -60 mV followed by a 250 or 300 pA current step or

### Explaining the effect of somatic current isolation with simulations

Somatodendritic Nav channel distribution was manipulated in a compartmental SN DA neuron model to investigate the mechanism by which somatic isolation of Nav channels results in an abnormally high pacemaker frequency. As noted (see Materials and Methods), the following analysis was not affected by the presence of an axon, AIS, or calcium-activated SK potassium channels. Somatic and dendritic current-clamp recordings (Fig. 1C) were simulated with Nav channels both evenly distributed throughout the somatic and dendritic compartments and isolated to the soma only. In this way, simulation mimicked control pre-TTX slice recordings and post-TTX dynamic clamp slice recordings. When Na<sub>V</sub> channels were distributed (Fig. 9A, left), full height APs were produced in both compartments with a slow frequency similar to that observed under similar somatic recording conditions in control slice recordings (Fig. 8A, top trace). However, simulating the dynamic clamp protocol by injecting Nav currents into the soma resulted in a threefold increase in somatic spiking frequency when compared with the distributed channel (Fig. 9A, top). Furthermore, simulated dendritic recordings revealed that the full height dendritic APs observed with distributed Nav channels were replaced by short, broad spikelets when the channels were isolated to the soma (Fig. 9A, bottom). These simulations suggest that the dendrites are essentially passive in the absence of local Nav channels and become a current sink due to the necessity to charge the capacitive load of the dendritic membrane (Fig. 9B,C). An imbalance between local Na<sub>V</sub> and K<sub>V</sub> currents then results in excess subthreshold current during the ISI, which in turn produces faster DP of the somatic and proximal membranes leading to faster pacing (compare Figs. 1*C*, middle, 9*C*).

## Simulation predictions for effects of manipulating $\mathrm{Na}_{\mathrm{v}}$ gating properties

If the model captures the true behavior of DA neurons, then it should also predict experimental responses to changes in virtual channel gating. One way to reduce local current could be to modify voltage-dependent gating to decrease the window current that tonically flows within a range of membrane potentials where steady-state activation and inactivation overlap (Fig. 1B, hatched area). Therefore, with soma-confined  $\mathrm{Na}_{\mathrm{V}}$  channels, three changes to  $Na_V$  gating parameters (Fig. 10A) were examined in the compartmental SN DA neuron model. First, to decrease the overall window current the activation curve  $(m_{\infty}^{3})$  was shifted 5 mV to the right and the inactivation curve  $(h_{\infty})$  was shifted 5 mV to the left (Fig. 10A; m/h shift). Even though more conductance was needed to produce normal height APs (3900 nS vs 800 nS), when the m/h shifted channel was substituted in the model the simulated firing frequency was slower (Fig. 10B; 3 Hz with m/hshift vs 5.5 Hz with Na<sub>v</sub>). Then, to isolate which gating parameter reduced the firing frequency, each parameter was shifted separately. Shifting only the activation curve 5 mV to the right (Fig. 10A; m shift) also required more conductance to produce normal height APs than native Na<sub>V</sub> and decreased spiking frequency (Fig.

30 nS virtual NMDA conductance. *A*, Representative traces of the first AP evoked by 250 pA current injection (top) under control conditions (control) and 100 nS of virtual anti-Na<sub>v</sub> channel conductance (-100 nS gNa<sub>v</sub>) and their corresponding dV/dt (middle) and phase plane (bottom) plots. Representative current-clamp recordings in response to (*B*) a 300 pA current injection and (*C*) 30 nS of virtual NMDA conductance under control conditions (control) and in the presence of 100 nS virtual anti-Na<sub>v</sub> channel conductance (-100 nS gNa<sub>v</sub>).



**Figure 7.** Na<sub>v</sub> current regulates the slow pacemaker rate of SN DA neurons. Representative current-clamp recordings (*A*–*C*, top) from freely pacing SN DA neurons to which (*A*) 200, (*B*) 100, and (*C*) – 100 nS of virtual Na<sub>v</sub> conductance have been added using dynamic clamp. The bottom graphs of *A*–*C* indicate the dynamic clamp current. *D*, Linear regression of the pacing frequency in response to different virtual Na<sub>v</sub> conductance levels. *E*, Second and third AP (top) and corresponding virtual Na<sub>v</sub> current (bottom) during the 200 nS gNa<sub>v</sub> application (*A*) to illustrate the additional Na<sub>v</sub> current added during the ISI.

10*B*; 2900 nS; 3 Hz). However, shifting only the inactivation curve 5 mV to the left (Fig. 10*A*; *h* shift) produced normal height APs with only a small increase in conductance (1100 nS vs 800 nS) and no change in spiking frequency (Fig. 10*B*; 5.5 Hz). Therefore, these simulations predict that only shifts in activation gating would normalize the spiking frequency when all Na<sub>V</sub> current is confined to the soma.

# Experiments conform to the model's predictions about channel activation

The model-generated hypothesis that high spiking frequency is induced by somatic channels as a consequence of excess somatic and proximal Na<sub>V</sub> current was tested by replacing native Na<sub>V</sub> currents blocked by 1  $\mu$ M TTX with virtual Na<sub>V</sub> channels that had altered gating parameters (i.e., as modeled above). The response to 50 pA current injections in neurons current-clamped at -60mV was then determined. For each modified virtual channel, conductance levels were adjusted to produce AP height that was at least 80% of the control (Fig. 11*B*). Under these conditions, *m/h* shift and *m* shift models produced lower spiking frequencies (Fig. 11*A*, *C*). However, the *h* shift model, like the unmodified virtual channel, produced abnormally fast activity (Fig. 11*A*, *C*). Therefore, as predicted by modeling (Fig. 10), only manipulations that reduced subthreshold Na<sub>V</sub> by shifting activation produced slower spiking when limited to the soma (Fig. 11*A*, *C*). This result shows that subthreshold  $Na_v$  current is important in regulating the pacing frequency in DA neurons.

#### Pacemaker frequency and somatod endritic $\mathrm{Na}_\mathrm{V}$ channel distribution

The experiments thus far examined the effect of changing  $Na_V$ channel density in the soma and eliminating Nav channels in dendrites. However, because DA neurons possess multiple dendrites, it is not possible to alter Nav channel density uniformly and simultaneously throughout the dendritic compartment with the dynamic clamp. However, the above analysis demonstrated the predictive power of modeling, in which it is possible to control compartmental channel distribution. Therefore, simulations were used to vary the balance of somatic and dendritic Nav channels to understand how distribution affects spiking frequency in DA neurons. Specifically, recordings of responses to 80 pA injections into the soma of neurons current-clamped to -60 mV were simulated with varying distributions of Nav channels in the soma and dendrites while keeping the total across both compartments a constant. Strikingly, as gNa<sub>V</sub> is moved from the soma to the dendrites, spiking frequency decreases (Fig. 12A, B). The plot of frequency dependence in Figure 12B shows that the uni-



**Figure 8.** Replacing the distributed native  $Na_v$  current with virtual  $Na_v$  current reconstitutes pacing, but at a higher frequency. *A*, Representative SN DA neuron current-clamp recording held at -60 mV followed by a 2 s long, 50 pA current injection before (pre-TTX; top trace) and after maximal block of TTX-sensitive sodium channels with 1  $\mu$ m TTX (second trace) followed by application of 600 nS (third trace) and 800 nS (fourth trace) of virtual  $Na_v$  conductance to the soma. *B*, AP height and (*C*) pacing frequency before TTX application (Native) and after 10 min of 1  $\mu$ m TTX application with different levels of virtual  $Na_v$  conductance. Error bars indicate the mean and SEM of 3–9 cells. *D*, Representative current-clamp recordings from a freely pacing neuron before and after 1  $\mu$ m TTX followed by reconstitution of pacing with 800 nS of virtual  $Na_v$  conductance.

form distribution found in native DA neurons produces a minimal pacemaker rate, while preserving somatic channels. In SN DA neurons, the preservation of somatic channels is critical for reliable backpropagation of APs through the soma into other nonaxon-baring dendrites and concomitant release of DA.

Modeling was also used to determine the effect of adding  $gNa_V$  to different compartments in neurons with an initially uniform distribution of  $Na_V$  channels (i.e., as found in native neurons). Strikingly, although the dendritic compartment is far larger than the soma, adding extra channels to the soma alone is as effective in increasing pacemaker frequency as distributing the extra channels throughout the dendrites or the whole somatodendritic compartment (Fig. 12*C*). This finding further emphasizes the critical role of  $Na_V$  channels in nigral DA neuron pacemaker frequency.

#### Discussion

Nav channels of SN DA neurons are known to be responsible for AP initiation in the AIS and propagation throughout the axonal, somatic and dendritic compartments. Although it has been suggested that Nav channel inactivation and density contribute to the susceptibility of DA neurons to DP block (Kuznetsova et al., 2010), a phenomenon that correlates with antipsychotic drug efficacy (Chiodo and Bunney, 1983; White and Wang, 1983a,b; Grace and Bunney, 1986; Esposito and Bunney, 1989; Skarsfeldt and Perregaard, 1990; Skarsfeldt, 1992; Valenti et al., 2011), this hypothesis has not been confirmed directly in neurons. Furthermore, it has also been unclear whether Na<sub>V</sub> channels in the soma play a role in controlling DA neuron pacemaker activity and DP block. Indeed, one might conclude that somatic channels are not critical because APs that initiate in the AIS coming off of a dendrite sometimes fail to backpropagate through the soma (Gentet and Williams, 2007) even though isolated somata can pace autonomously (Kita et al., 1986; Hainsworth et al., 1991). In this study, dynamic clamp was used to show that, even though APs initiate in the AIS, somatic Nav channels contribute to pacemaker frequency and susceptibility to DP block. It was also shown that limiting Nav channels to the soma is sufficient for pacemaker activity, but this produces abnormally high frequencies due to excessive local subthreshold Na<sub>V</sub> current. Although not confirmed by direct measurement of dendritic voltage, these results together with computational modeling provide evidence that the slow pacemaker frequency that characterizes SN DA neurons is supported by the wide distribution of Nav channels in the somatodendritic compartment. A secondary consequence of low Na<sub>V</sub> channel density, compared with fast pacing neurons, is that SN DA neu-

rons are susceptible to DP block. Thus, two seemingly separate characteristics, low-frequency pacemaker activity and susceptibility to DP block, are causally linked to  $Na_V$  channel density and localization in SN DA neurons.

This Na<sub>v</sub> channel balancing act between firing frequency and DP block susceptibility may be a general principle. If this is the case, then neurons with high Na<sub>v</sub> channel densities should exhibit high firing frequencies and a reduced sensitivity to DP block. In fact, this is observed in GABA neurons of the SN pars reticulata. These neurons express a similar complement of Na<sub>v</sub> channel pore forming  $\alpha$ -subunits and auxiliary  $\beta$ -subunits as DA neurons, but have a higher Na<sub>v</sub> channel density and produce faster pacemaker activity (Seutin and Engel, 2010; Ding et al., 2011). These cells are also relatively more resistant to DP block than SN DA neurons (Richards et al., 1997). Thus, Na<sub>v</sub> channels

may influence both pacemaker frequency and susceptibility to DP block in a variety of neurons.

An alternative case of somatodendritic Nav density, distribution, and gating occurs in serotonergic (5-HT) medullary raphé (MR) neurons, which exhibit slow pacemaker activity (Wang and Richerson, 1999) with broad APs (Zhang et al., 2006) like SN DA neurons. Both DA and 5-HT neurons produce somatodendritic neurotransmitter release, but with different mechanisms resulting in the necessity for differential channel distribution and density. In SN DA neurons, APs backpropagate into the distal dendrites with very little decrement resulting in Nav channel-dependent dendritic release of DA (Santiago et al., 1992; Häusser et al., 1995). However, in 5-HT neurons in the dorsal raphé nucleus, dendritic activity-dependent calcium signals decrement with distance from the soma (de Kock et al., 2006) and release of 5-HT from dendrites (unlike from the soma) is AP independent (L. Colgan and E. Levitan, personal communication). Furthermore, consistent with our analysis and the more limited contribution of dendritic Nav channels in 5-HT neurons, pacemaker activity was reconstituted with somatic virtual Nav channels in 5-HT MR neurons, but no gating adjustment was needed to achieve the slow pacemaker rate (Milescu et al., 2010). Therefore, it is likely that 5-HT MR neurons have few dendritic Na<sub>v</sub> channels relative to the soma, thus producing different somatodendritic excitability and release than found with DA neurons.

In DA neurons, the slow pacemaker activity that results from low Nav channel density and broad somatodendritic distribution may be of importance for sensitivity to behaviorally relevant stimuli. DA neuron intrinsic pacemaker activity contributes to setting the dopaminergic tone of target brain regions. Synaptic activity modifies the intrinsic pacemaker activity of SN DA neurons to produce behaviorally relevant regular, irregular, and bursting patterns of activity (Hyland et al., 2002). Burst firing results in a larger DA release than baseline activity (Heien and Wightman, 2006). It is this differential DA release that indicates the potential reward value of a particular stimulus (for review, see Hauber, 2010). Putzier et al. (2009b) showed that the response of SN DA neurons to both inhibitory and stimulatory synaptic input depends exponentially on the baseline ISI of the neuron (i.e., the slower the baseline frequency the larger the potential response). Therefore, if so-



**Figure 9.** Somatic isolation of Na<sub>v</sub> current results in abnormally fast pacing in an SN DA neuron compartmental model. The simulation paralleled the experimental protocol shown in Figure 7. *A*, Simulated voltage traces with distributed and somatically isolated Na<sub>v</sub> in response to an 80 pA applied current pulse measured from the soma and dendrite. *B*, Diagram of Na<sub>v</sub> currents flowing in a simplified somatodendritic compartment with Na<sub>v</sub> channels distributed (left) or in the soma only (right). When Na<sub>v</sub> channels are distributed, Nav currents can uniformly activate Kv channels resulting in little axial current flow (left). When all of the gNaV is in the soma, the sodium current spreads axially, depolarizing the distal regions much less than the proximal regions, resulting in a proximal to distal Kv current gradient. Large arrows indicate axial current sink. *C*, Somatic currents flowing during the ISI of spikes 6 and 7 in the Soma Only gNa<sub>v</sub> condition in *A*.  $I_{Kv}$  = composite voltage-gated potassium currents,  $I_b$  = sum of constitutively active GIRK current and sodium leak current,  $I_{cav,L}$  = L-type calcium current,  $I_{nav}$  = TTX-sensitive voltage-gated sodium current, and  $I_{Axial}$  = axial current.  $I_{Axial}$  and  $I_{Nav}$  have been plotted separately on the right graph with an expanded *y*-axis scale. For comparison, see the middle panel of Figure 1C for the ISI somatic currents flowing during the distributed gNa<sub>v</sub> condition.



**Figure 10.** Simulations predict effects of Na<sub>v</sub> window current manipulations on spiking frequency. *A*, Steady-state inactivation and activation curves of the model Na<sub>v</sub> current (solid lines in each graph), a 5 mV right shift in the activation curve and a 5 mV left shift in the inactivation curve (*m/h* shift; dotted lines; top), a 5 mV right shift in the activation curve only (*m* shift; dotted line; middle), and a 5 mV left shift in the inactivation curve (*h* shift; dotted line; bottom) used in both dynamic clamp and modeling experiments. Shaded area of each inset indicates the resulting window current for each manipulation. *B*, Simulated activity of a model SN DA neuron held at -60 mV and stimulated with a 2 s, 80 pA current injection with somatically isolated Na<sub>v</sub> current with the indicated gating shifts.

matodendritic balance of  $Na_v$  current were modified, the resulting change in of baseline frequency could reduce the potential responsiveness of the neuron to synaptic input.

Na<sub>V</sub> channel current kinetics, expression, and targeting are endogenously modulated by transcriptional and posttranslational modifications, protein–protein interactions, and differences in Na<sub>V</sub>  $\alpha$ - and  $\beta$ -subunit composition (Diss et al., 2004; Shao et al., 2009). These changes can occur acutely, within seconds to minutes in the case of phosphorylation events, or chronically, within hours to days as with protein expression and changes in trafficking. Therefore, these mechanisms for regulating somatic Na<sub>V</sub> channels have the potential to modulate SN DA neuronal pacemaker frequency and thus sensitivity to synaptic input.

Somatic  $Na_V$  channel modulation may also have the potential to affect the neuroleptic effects and extrapyramidal side effects of some antipsychotic drugs. The clinical efficacy and side effects of chronic antipsychotic drug treatment have been correlated with DP block of midbrain DA neurons recorded in chronically treated anesthetized animals (Chiodo and Bunney, 1983; White and Wang, 1983a,b; Grace and Bunney, 1986; Esposito and Bunney, 1989; Skarsfeldt and Perregaard, 1990; Skarsfeldt, 1992; Valenti et al., 2011). Recently, antipsychotic drugs were shown to accumulate in neurons and be released to inhibit Na<sub>v</sub> channels (Tischbirek et al., 2012). The results presented here suggest that this inhibition could, by reducing somatic Na<sub>v</sub> channel activity, contribute to DP block and hence the efficacy of antipsychotic drugs.

In conclusion, the proper distribution and density of Nav channels throughout the soma and dendrites of SN DA neurons is necessary for the hallmark slow pacemaker rate, which allows for optimal differential DA release upon synaptic stimulation of SN DA neurons. Furthermore, the low somatic Nav channel density responsible for the characteristic slow pacemaker activity of SN DA neurons is also responsible for their susceptibility to DP block, a characteristic of DA neurons linked to the efficacy of antipsychotic drugs. The balance of Nav channels required for optimal pacemaker frequency and sensitivity to DP block can be tipped by changing the Nav current density, distribution, or gating, which could result in altered signal transmission and antipsychotic drug efficacy.

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**Figure 12.** Simulation predictions of frequency with differential somatodendritic Na<sub>v</sub> channel distribution. *A*, Simulated activity of model SN DA neuron held at -60 mV and stimulated with a 2 s, 80 pA current injection, and 845 nS of gNa<sub>v</sub> was distributed across the 23.75 pF of the  $C_m$  of the soma and the 191.31 pF  $C_m$  of the dendrites at varying ratios. The traces in *A*, from top to bottom, have the following somatic/dendritic Na<sub>v</sub> current densities in nS/pF: Soma Only = 35.6/0, Soma 8× > Dendrite = 17.8/2.2, Soma 2.5× > Dendrite = 8.4/3.4, Soma = Dendrite = 3.9 uniformly distributed, and Dendrite Only = 0/4.4. *B*, Spiking frequency as a result of changing the percentage distribution of 845 nS of gNa<sub>v</sub> between the soma and dendrites in the DA neuron compartmental model as demonstrated in *A*. *C*, Simulated current-clamp recordings from a pacing model neuron to which 200 nS of gNa<sub>v</sub> was added to the soma (top), uniformly distributed (middle), or added to the dendrites only (bottom).

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